

DEVICES AND METHODS FOR TREATING VASCULAR MALFORMATIONS

BACKGROUND OF THE INVENTION

5 The present invention relates to treatment of abnormalities in a patient's vascular system. A specific use of the present invention described below is for the treatment of cerebral aneurysms although the various aspects of the invention described below may also be useful in treating other abnormalities such as arteriovenous malformations (AVM), hypervascular tumors, cavernous carotid fistulas, fibroid tumors, and non-reversible sterilization via fallopial occlusion.

10 Cerebral aneurysms are enlargements of the cerebral vasculature which protrude like a balloon from the wall of a cerebral artery. The cerebral aneurysm has a neck which leads to the parental vessel and a body or "dome" which can vary in diameter from 1-30 mm.

15 The wall of the aneurysm is often weak and can rupture, leading to hemorrhage. Rupture of the aneurysm can kill the patient or leave the patient with permanent or transitory mental and physical deficits.

20 Aneurysms are often treated to prevent rupture, leading to hemorrhage, or to prevent rebleeding of acutely ruptured aneurysms. A conventional method of treating aneurysms is to fill the aneurysm with coils. The coils are introduced into the aneurysm one at a time through a delivery catheter until the aneurysm is filled. The aneurysm eventually becomes a solid mass of coils and thrombus.

25 A problem with the conventional method of using coils to fill aneurysms is that the aneurysm becomes a relatively solid mass due to coils and thrombus contained therein. The mass of coil and thrombus exerts pressure on adjacent areas of the brain which may lead to other problems. Another problem with the conventional method is that the coils must be delivered one at a time into the aneurysm which increases the procedure time and risk to the patient. For large aneurysms, up to twenty coils may be required to fill the aneurysm.

30 It is an object of the invention to provide improved methods and devices for treating aneurysms. These and other objects of the invention will become evident from the description of the preferred embodiments described below.

SUMMARY OF THE INVENTION

In a first aspect of the present invention, a method of treating an aneurysm is provided. An expandable structure is delivered through the vasculature in a collapsed position. Once the expandable structure is at the desired location, such as within a cerebral aneurysm, the expandable structure is expanded. The structure and advantages of the expandable structure are described below. The aneurysm wall is also reduced in size so that the aneurysm does not need to be completely filled in the conventional manner. The expandable shape is sized to be smaller than the aneurysm to permit reducing the size of the aneurysm by at least 30% percent.

A preferred method of reducing the size of the aneurysm is to heat the aneurysmal wall, preferably to a temperature of at least 60° and preferably 60-80°C, which causes the aneurysmal wall to shrink. The aneurysm may be heated in any suitable manner and preferred methods are monopolar and bipolar RF, laser, microwave, and simple electrical resistance heating. In a preferred method, electrical energy is delivered to the expandable device itself to generate heat. A fluid may be introduced into the aneurysm to prevent clotting during heating and to provide thermal and/or electrical conductance. When using RF heating, for example, the fluid may be saline and more preferably hypertonic saline. Although it is preferred to heat the aneurysmal wall to reduce the size of the aneurysm, the aneurysm may also be reduced in size by chemical action.

The expandable structure forms a matrix of filaments in the expanded condition. The matrix preferably forms a woven or braided structure, however the filaments may also be randomly oriented, parallel, or non-intersection filaments. The matrix may be flexible filaments, such as platinum ribbon, extending randomly, radially or helically within an expandable, permeable, mesh-like enclosure. The material may also be an expandable material such as polymer, nitinol, stainless steel, tungsten or tantalum and alloys/composites thereof.

The expandable device preferably fills a volume of at least 10% of the aneurysm volume, more preferably at least 40% and most preferably at least 60% of aneurysm volume. The expandable device preferably has internal filaments within the volume to quickly form a stable thrombus. An advantage of the expandable device is that a three-dimensional structure forms without requiring separate delivery of a cage and coils as described in International Application WO 99/07293. In another aspect, the expandable device has a deforming portion which plastically deforms when moving to the

expanded position. The deformable portion holds the flexible filaments in the expanded position.

The aneurysm may be reduced in size until the aneurysmal wall contacts the expandable structure so that the expandable structure supports and reinforces the aneurysmal wall. In a particularly advantageous embodiment of the invention, the expandable structure itself is used to transmit energy to heat the aneurysmal wall which causes the aneurysmal wall to fuse to the expandable structure, thereby reinforcing the aneurysmal wall and preventing migration of the expandable structure into the parental vessel.

In another aspect of the invention, the aneurysmal wall may be reduced in size together with the expandable device. In a preferred embodiment, the expandable structure is a soft mesh which easily collapses when the aneurysmal wall is shrunk.

Various optional steps and structure may also be provided. For example, a sealant may be delivered into the aneurysm to ensure that the aneurysm is isolated from the parental artery. An advantage of the present invention is that the sealant is held within a matrix formed by the expandable device which holds the sealant in the aneurysm.

The proximal portion of the expandable structure may be insulated to protect the neck of the aneurysm. The insulation may coat only the flexible filaments so that the structure is still permeable to fluid. Alternatively, the insulation may be impermeable to protect the neck from hot fluid slowly expelled into the aneurysm or to isolate the aneurysm entirely from the parental vessel.

The expandable device may have one or more expandable sections. In an embodiment, the expandable device has two expandable sections wherein energy is delivered to the dome with one of the sections while the second section is insulated to protect the neck.

The expandable device may have a locking mechanism for locking the expandable device in the expanded position. The expandable device is naturally biased toward the collapsed position so that the operator may partially deploy the expandable device to determine whether the device has the appropriate size. If the device does not have the appropriate size, the device is collapsed and removed and another device having the appropriate size is introduced. The locking mechanism is then actuated when the user is satisfied with the size of the device.

In still another aspect of the present invention, a catheter has a cover which is positioned over the neck of the aneurysm to isolate the aneurysm from the parental vessel. The aneurysm is then reduced in size as explained above while the cover isolates the aneurysm. The cover also protects the patient from hemorrhage by isolating the aneurysm from the parental vessel. The cover may be periodically moved to expel heated fluid into the parental vessel when heating and shrinking the aneurysm.

In yet another aspect of the present invention, a coil is used to cover the neck of the aneurysm to regulate the flow of hot fluid out of the aneurysm and into the parental vessel. The pitch of the coil can be varied by the operator during deployment to allow faster or slower leakage of hot fluid out of the aneurysm and into the parent artery during heating.

A catheter is also provided which has a low-impedance coil, such as flat copper ribbon or other suitable material, disposed in the catheter tip. Upon infusion of saline through the catheter and passage of RF energy through the coil, the saline is heated and conducts electrical energy to heat the fluid.

These and other aspects and advantages of the invention will become evident from the following description, drawings and claims.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig. 1 is a system for treating a patient's vascular system.

Fig. 2 shows an expandable device in a collapsed position.

Fig. 3 is a perspective view of the expandable device with the mesh removed.

Fig. 4 is a cross-sectional view of the expandable device.

Fig. 5 shows the expandable device in an aneurysm.

Fig. 6 shows the expandable device detached from the delivery catheter.

Fig. 7 shows the expandable device of Fig. 6 with a sealant introduced into a portion of the expandable device.

Fig. 8 shows the sealant filling the aneurysm and the expandable device.

Fig. 9 shows the expandable device having a proximal portion which is relatively impermeable to the sealant so that the sealant is retained in the aneurysm.

Fig. 10 shows the expandable device filled with an expandable material such as random fibers or a coil.

Fig. 11 shows another expandable device which is deployed with a balloon in a collapsed position.

Fig. 12 shows the expandable device of Fig. 11 in an expanded position.

Fig. 13 shows the expandable device reduced in size and the expandable device having a proximal portion which is insulated to protect the neck of the aneurysm.

Fig. 14 shows the expandable device of Fig. 11 with simple resistance heating used to shrink a portion of the aneurysm into contact with the expandable device.

Fig. 15 shows the use of simple resistance heating to shrink another portion of the aneurysm into contact with the expandable device.

Fig. 16 shows a heating device.

Fig. 17 shows a heating device with the tip curved.

Fig. 18 shows the heating device used with the expandable device of Figs. 11-14.

Fig. 19 shows the aneurysm shrunk into contact with the expandable device.

Fig. 20 shows the expandable device reduced in size during shrinking of the aneurysm.

Fig. 21 shows another expandable device having a locking mechanism for holding the device in the expanded position.

Fig. 22 shows the expandable device of Fig. 21 with the device in the expanded position.

Fig. 23 shows the device of Figs. 21 and 22 released from the delivery catheter.

Fig. 24 shows a catheter having a cover for isolating an aneurysm from the parental vessel.

Fig. 25 is a cross-section of the catheter of Fig. 21 along line A-A.

Fig. 26 shows the catheter of Fig. 21 with the cover having a curved shape.

Fig. 27 shows the catheter of Fig. 21 isolating an aneurysm.

Fig. 28 shows the aneurysm reduced in size and a thrombogenic material and sealant introduced into the aneurysm.

Fig. 29 shows only the thrombogenic material in the aneurysm.

Fig. 30 shows another expandable device in a collapsed position.

Fig. 31 shows the expandable device of Fig. 30 in an expanded position.

Fig. 32 is an alternative embodiment of the device of Figs. 30 and 31.

Fig. 33 is another alternative embodiment of the device of Figs. 30 and 31.

Fig. 34 shows a mesh structure for use with any of the expandable devices described herein.

Fig. 35 shows a number of expandable device delivered to the aneurysm.

5 Fig. 36 shows the aneurysm of Fig. 35 reduced in size.

Fig. 37 shows a coil for regulating flow between an aneurysm and a parent vessel.

Fig. 38 shows the coil of Fig. 37 with the windings spaced close together to further impede fluid flow between the aneurysm and the parent vessel.

10 Fig. 39 shows another catheter for heating tissue.

Fig. 40 is a cross-sectional view of the distal end of the catheter of Fig. 39.

Fig. 41 shows the tip of the catheter of Figs. 39 and 40 with holes at the distal end of the tip.

15 Fig. 42 shows the tip of the catheter of Figs. 39 and 40 with holes along the side of the tip.

DESCRIPTION OF THE SPECIFIC EMBODIMENTS

Referring to Fig. 1, a system 2 for introducing an expandable device 4 into a cerebral aneurysm is shown. A first catheter 6 extends through a penetration in the femoral artery and up to the carotid artery. A second catheter 8 is advanced through the first catheter 6 and into the cerebral vasculature to the site of the aneurysm or other abnormality. A delivery catheter 10 is then advanced through the second catheter 8. The catheter 10 delivers an expandable device 4 which partially fills the aneurysm as will be described below. The system 2 also has an energy supply 12 for heating the aneurysm to shrink the aneurysm as will be described below.

25 After the expandable device 4 has been delivered to the aneurysm and expanded, the aneurysm is reduced in size as shown in Fig. 6. The aneurysm may be shrunk partially toward the expandable device 4, into engagement with the expandable device 4, or may even be shrunk until the expandable device 4 is also reduced in size. An advantage of shrinking the aneurysm is that the aneurysm does not need to be completely
30 filled with coils in the conventional manner. The conventional method of filling the aneurysm with coils creates a relatively solid mass in the aneurysm which can press against adjacent structures leading to further problems. The expandable device 4 is removably mounted to the end of a shaft 5 in the manner described below so that the

expandable device 4 may be released in the aneurysm. The expandable device may be released with a mechanical mechanism, a thermoadhesive bond, or an electrolytically or chemically severable bond.

5 The aneurysm may be shrunk in any suitable manner and a preferred method is to heat the aneurysmal wall. Shrinking of the aneurysm may also be accomplished through chemical action. The aneurysmal wall is preferably heated to a temperature of 60-80°C and preferably at least 70°C. Depending upon the size of the aneurysm, the aneurysmal wall is preferably heated for at least 10 seconds and generally between 10 seconds and 5 minutes.

10 In the preferred system of Fig. 1, the energy supply 12 supplies RF energy to heat and shrink the aneurysm. The expandable device 4 is preferably configured as a mono-polar RF electrode 14 and the energy supply 12 is preferably an RF generator. A suitable second electrode (not shown) is placed in contact with the patient's skin in the conventional manner. The aneurysm may, of course, be heated with the energy supply
15 being a hot fluid, laser, microwave, bi-polar RF or a resistance heating device without departing from the scope of the invention.

Referring to Figs. 1 and 4, the catheter 8 has a lumen 16 coupled to a source of fluid 18 which is preferably a conductive fluid such as saline and more preferably hypertonic saline. The lumen 16 may also be coupled to a source of sealant 20
20 which may be used to seal the aneurysm as described below. The sealant may be any suitable sealant such as cyanoacrylates, ethylene vinyl-alcohol, cellulose acetate polymers, fibrin glues and other liquid-type tissue sealants. The sealants may also be bioperodable and/or bio-absorbable. The lumen 16 is also coupled to a vacuum source 22 for suctioning fluids and reducing the size of the aneurysm. A source of contrast 24 is
25 also provided for visualization of the aneurysm, vasculature and device positions. A valve 26 couples the lumen 16 to the various sources 18, 20, 22, 24. The delivery catheter 10 also has a lumen 28 which may be coupled to the sources 18, 20, 22, 24 and discussion of use of the lumen 16 is equally applicable for the lumen 28.

Referring to Figs. 2, 3 and 5, the expandable device 4 has first and second
30 expanding sections 30, 32. Although it is preferred to provide both the first and second expanding sections 30, 32, the expandable device 4 may include only one expanding section or three or more expanding sections without departing from the scope of the invention. The first section 30 acts as the electrode 14 to deliver RF energy from the energy source 12 to the aneurysm. The second section 32 is insulated and does not

transmit energy to the aneurysm so that the neck of the aneurysm is protected. The second section 32 is preferably coated with PTFE, polyamide, FED, or PFA to prevent RF energy transmission. Protecting the neck of the aneurysm also protects peripheral vessels adjacent the neck of the aneurysm.

- 5 The second expandable section 32 may be permeable to fluid so that heated fluid in the aneurysm may be slowly expelled into the parental vessel to dissipate heat. The second section 32 may also have a fluid impermeable portion 36 adjacent the neck to further protect the neck of the aneurysm as shown in Fig. 9. The fluid impermeable portion 36 is preferably a flexible sheath 38 having a ring or annular shape.
- 10 The ring shape may interrupted at a radially inner portion 39 so that heated fluid may still be slowly expelled into the parental vessel. Alternatively, the sheath 38 may completely isolate the aneurysm from the parental vessel.

- The first and second expandable sections 30, 32 have a number of flexible filaments 40 which move from the collapsed position of Fig. 2 to the expanded position of
- 15 Fig. 5. The flexible filaments 40 are preferably woven or braided to form a substantially closed-form mesh structure 42 in the expanded position. The filaments 40 and mesh 42 have the characteristics described below and are graphically depicted in the drawings for clarity. A preferred mesh structure 42 is also described with reference to Fig. 34 below.

- Referring again to Figs. 2 and 3, the filaments 40 are positioned over
- 20 deformable elements 48 which hold the flexible filaments 40 in the expanded position. Referring to Fig. 3, the deformable elements 48 have columns 50 extending between collars 52, 53 at the ends. The deformable elements 48 are formed from tubes which have four cut-out sections 54 to form the columns 50. The collars 52 are then attached to the ends of the tube. The columns 50 are bent outward slightly so that they will buckle
- 25 outwardly when compressed. As will be described in further detail below, the deformable elements 48 are plastically deformed when moving to the expanded position to hold the filaments 40 in the expanded position. The columns 50 may also be designed with curved or sinusoidal shaped sections to improve flexibility.

- Referring to Fig. 4, the proximal and distal collars 52 are threaded to
- 30 engage a threaded tip 58 of a guidewire 60 for manipulating the expandable device 4. Intermediate collars 62 provide only throughholes to hold and guide the expandable device 4 on the guidewire 60. When expanding the device 4, the guidewire 60 is pulled until the device 4 is trapped between the delivery catheter 10 and the threaded tip 58. The guidewire 60 is then rotated to engage the tip 58 with the distal threaded collar 52. When

the tip 58 is threaded into engagement with the distal collar 52, the guidewire 60 can be pulled to expand the device. When the device 4 is partially expanded, the deformable elements 48 may still be within their elastic range so that the expandable device 4 will recover the collapsed position when tension is released on the guidewire 60. The operator may then check to see if the device 4 has the appropriate size and shape for the aneurysm before fully deploying the device. If the operator determines that the device 4 is too small or too large, the device 4 is collapsed and removed and another expandable device of appropriate size advanced to the aneurysm.

When the operator is ready to deploy the device 4, the operator pulls the guidewire 60 so that the deformable elements 48 undergo plastic deformation and move to the expanded position. Even if the device 4 is moved to the expanded position, the operator may still retrieve the device by engaging the proximal collar 53 with the threaded tip 58 and withdrawing the device into the second catheter 8.

After the expandable device 4 has been moved to the expanded position, the aneurysm is then preferably reduced in size. In a preferred method, RF energy is delivered to the first expandable section 30 through the guidewire 60 and a conductive fluid, preferably hypertonic saline, is injected into the aneurysm through the lumen 16 or lumen 28. Fig. 6 shows the aneurysm reduced in size until the aneurysm engages the first section 30. The threaded tip 58 is then disengaged from the device 4 leaving the device 4 in the shrunken aneurysm.

As an optional step, the sealant 64 from the source of sealant 20 may also be introduced into the entire aneurysm (Fig. 8) or into just the second section 32 (Fig. 7) to seal the aneurysm. An advantage of the present invention over conventional methods is that the sealant 64 is contained within the closed-form mesh structure 42 to prevent escape of the sealant 64 into the parental vessel. Referring to Fig. 9, a proximal portion 66 may be impermeable to further isolate the aneurysm from the parental vessel. A small amount of the sealant 64 may also be delivered to completely isolate the aneurysm if necessary as shown at dotted-line 68. The method of the present invention described above may, of course, be practiced with any suitable structure other than the structure of Figs. 1-9 without departing from the scope of the invention.

Referring to Figs. 11-15, another delivery catheter 70 is shown for use with the system of Fig. 1. The delivery catheter 70 is delivered through the first and second catheters described above. The catheter delivers an expandable device 4A to the aneurysm through the second catheter 8 (see Fig. 1).

The delivery catheter 70 has an expandable member 72, preferably a balloon 74, for deploying the expandable device 4A. The device 4A is configured to retain the expanded position of Fig. 12 after the balloon 74 has been deflated. The delivery catheter 70 has an inflation lumen 72 coupled to a source of inflation fluid 74 for inflating the balloon (Fig. 1).

The expandable device 4A is preferably made of a number of flexible filaments 76. The filaments 76 are preferably woven or braided but may also be a number of non-woven filaments. The filaments 76 may be any suitable material and a preferred material is platinum alloy (92% platinum, 8% tungsten) wire having a thickness of 0.005-0.003 inch.

The expandable device 4A may take any shape and may have a number of predetermined shapes which can be selected depending upon the shape of the aneurysm and the nature of the patient's vasculature. Referring to Fig. 12, the expandable device 4A has a simple spherical shape. Although the expandable device 4A is shown as spherical, the expandable device 4A preferably has a width to height ratio of more than 1.1, more preferably at least 1.2 and most preferably at least 1.8. The width and height are defined relative to the aneurysm (Fig. 12) and/or relative to a longitudinal axis 76 of the expandable device 4A. The preferred dimensions provide a relatively large width so that the expandable device 4A cannot escape through the neck of the aneurysm after expansion. The height of the expandable device 4A provides clearance for shrinking the aneurysmal toward the expandable device. The width to height ratios are preferred dimensions for all of the embodiments described herein.

Once the expandable device 4A has been delivered to the aneurysm, the aneurysm is preferably reduced in size in any manner described herein. A method of reducing the size of the aneurysm is to deliver energy to the expandable device 4A from the energy source 12. The energy may be delivered to the aneurysm by delivering RF energy to the expandable device 4A with one or more wires 80 passing through the second catheter 8. During RF delivery, the second catheter 8 may be used to deliver fluid, such as hypertonic saline, to the aneurysm.

Referring to Figs. 14 and 15, simple resistance heating may also be used by moving the wires 80 into contact with the expandable device 4A to conduct electricity therebetween as shown in Fig. 14. An advantage of the system is that different portions of the aneurysm can be heated to shrink the aneurysm as shown in Figs. 14 and 15.

The expandable device 4A may be insulated at a proximal portion 82 so that energy is delivered to the aneurysm dome rather than toward the neck and parental artery. The flexible filaments 76 may be coated with any suitable insulation, such as paroline, and may be applied by spraying, dipping or etching. The expandable device 5 4A may also have the flexible sheath 78 over the insulated region to further shield the neck of the aneurysm.

Referring to Fig. 16, a heating device 84 is shown which may be used to heat and shrink the aneurysm. The heating device 84 is advanced into the aneurysm to heat fluid in the aneurysm thereby heating and shrinking the aneurysmal wall. Two 10 insulated wires 86, 88 are wrapped around a core wire 90 and covered with a sheath 92 along the proximal portion. The sheath 92 forms a lumen 94 therethrough which may be coupled to the various sources 18, 20, 22, 24 described above with connector 96. The distal end of the wires 86, 88 form proximal and distal electrodes 98, 100 for bipolar RF heating. The core wire 90 is attached to the distal electrode 100.

15 An actuator 102 is manipulated to change the distance between the electrodes 98, 100 and to bend the tip in the manner shown in Fig. 17. The actuator 102 is coupled to the core wire 90. The device may be configured so that the electrodes 98, 100 move toward another when the actuator 102 is manipulated, or the device may be configured so that the tip curves as shown in Fig. 17. The tip may be curved to navigate 20 tortuous vessels and may be curved during heating. In use, the distal end of the device 84 is introduced into the aneurysm and the actuator 102 is manipulated to curve the distal end. RF energy is then delivered and a fluid, such as hypertonic saline, is delivered through the second catheter 8 or through the lumen 94.

Referring to Figs. 18 and 19, the aneurysm may be shrunk into contact 25 with the expandable device so that the expandable device 4A reinforces the aneurysmal wall to prevent rupture. The aneurysmal wall may also be shrunk further so that the expandable device 4A itself shrinks as shown in Fig. 20. After the aneurysm has been reduced in size, the sealant 64 may also be delivered to further seal the aneurysm.

Referring to Figs. 1 and 21-24, another delivery catheter 110 for treating 30 an aneurysm with the system 2 of Fig. 1 is shown. The catheter 110 is advanced to the carotid artery and the second catheter 8 is advanced through the first catheter 6 to the aneurysm. The delivery catheter 110 extends through the second catheter 8 to deliver an expandable device 4B to the aneurysm. The delivery catheter 110 has a lumen 112 which may be coupled to one or more of the various sources 18, 20, 22, 24. The expandable

device 4B is coupled to the energy source 12 for heating and shrinking the aneurysm as will be described below.

The expandable device 4B is movable from the collapsed position of Fig. 21 to the expanded position of Fig. 22. Flexible filaments 114 preferably form a woven or braided mesh structure 116 extending between first and second hubs 118, 120. A central post 122 extends from the second hub 120 and has a locking mechanism 124 which engages the first hub 118 to hold the expandable device 4B in the locked position. An actuator 126, which is preferably a tapered rod 128, has a threaded connection 130 with the central post 122. The actuator 126 is pulled to move the locking mechanism 124 into engagement with the second hub 120. The locking mechanism 124 has spring elements 126 which are naturally biased to the position of Fig. 23. The spring elements 126 are angled proximally so that they are displaced inwardly by the hub 118 when the post 122 and spring elements 126 pass through the hub 118. After the spring elements 126 have passed through the hub 118 they assume their unbiased shape thereby locking the device 4B in the expanded position. The locking mechanism 124 may be any suitable locking mechanism.

The flexible filaments 114 preferably bias the device 4B toward the collapsed position so that the operator may partially expand the device to determine whether the device has the appropriate size. If the device is not the appropriate size, the device can be collapsed and withdrawn through the second catheter 8. After the expandable device 4B has been expanded, the aneurysmal wall may then be shrunk in any manner described herein. In the preferred embodiment of Fig. 21, the expandable device is a monopolar RF electrode with the energy source being an RF generator coupled to the actuator 126. The expandable device 4B may be insulated along a proximal portion 116 to protect the neck, parental vessel and adjacent vessels as mentioned above. After the aneurysmal wall has been reduced in size, the sealant 64 (Fig. 8) may be introduced to isolate the aneurysm from the parental vessel.

In another aspect of the present invention, the expandable devices 4, 4A, and 4B may be filled with an expandable thrombogenic material 130. Referring to Fig. 10, the expandable device 4 is filled with the compressible, thrombogenic material 130 which may be randomly oriented fibers 132 or coils 134. When the expandable device 4 is expanded, the material 130 expands to occupy the interior volume of the woven or braided mesh structure 42. The material 130 may be used with any of the expandable devices described herein without departing from the scope of the invention.

When the material 130 includes filaments 136, the filaments 136 may be helically, radially or randomly oriented within the interior volume of the mesh or braided structure 42.

Referring to Figs. 1 and 24-27, another catheter 140 for treating an aneurysm with the system of Fig. 1 is shown. The first catheter 6 is introduced through the femoral artery and advanced to the carotid artery. The second catheter 8 is advanced through the first catheter 6 to the aneurysm. The delivery catheter 140 is passed through the second catheter 8 to the aneurysm to treat the aneurysm.

The delivery catheter 140 has a lumen 142 which is coupled to the sources of fluid, contrast, sealant and vacuum 18, 20, 22, 24. The distal end of the catheter 140 has a cover 144 which is positioned over the neck of the aneurysm as shown in Fig. 27. The cover 144 provides temporary isolation of the aneurysm from the parental vessel. The cover 144 is preferably a disc of relatively soft material such as silicone. The cover 144 is preferably configured to cover an area of about 0.8 mm^2 to 75 mm^2 and is relatively thin so that the cover 144 does not impede flow through the parental vessel and so that the cover 144 can distort to a small profile when passing through the second catheter 8. The cover 144 is also preferably impermeable so that the cover 144 can isolate the aneurysm from the parental vessel.

The catheter 140 has an electrode 146 which is coupled to the energy source 12 with a wire 148 extending through the catheter 140. The electrode 146 may be configured as a monopolar RF electrode for delivery of RF energy with a second electrode (not shown) in contact with the patient's skin. Alternatively, a second electrode 150 may be passed through the lumen 142 to provide monopolar or bipolar RF with the first and/or second electrodes 146, 150. Shrinking of the aneurysm may, of course, be accomplished with any of the methods described above. For example, the heating device 84 (Fig. 16) may be advanced through the lumen 142 to heat and shrink the aneurysm.

Use of the delivery catheter 140 is now described, the delivery catheter 140 is advanced through the second catheter 8 to the aneurysm. The cover 144 is positioned over the neck of the aneurysm and the aneurysm is heated to shrink the aneurysm. When using RF heating, fluid such as hypertonic saline may be infused into the aneurysm through the catheter 140 or second catheter 8 (Fig. 1). The cover 144 may be flexible enough to deflect and permit hot fluid to be slowly expelled into the parental vessel. Alternatively, the cover 144 may be periodically moved away from the neck so that hot fluid in the aneurysm may be slowly expelled into the parental vessel. The

aneurysm may be reduced to an acceptable size or partially shrunk and filled with the thrombogenic material 130 and sealant (Fig. 28) or just the material 130 (Fig. 29).

Although the delivery catheter 140, and particularly the cover 144, have been described in connection with RF delivery, the cover 144 may be incorporated into any of the other catheters described herein or any other catheter without departing from the scope of the invention.

Referring to Figs. 30-34, another expandable device 160 is shown for use with the system of Fig. 1. The expandable device 160 is advanced through the second catheter 8 with a delivery catheter 162. The expandable device has a mesh 166 which covers a spring 160 made of a shape memory material. The expandable device 160 is in the collapsed shape of Fig. 30 when advanced through the second catheter 8. After the expandable device 160 is within the aneurysm, a wire 161 or other device can be advanced to contact the device 160 to heat the device and the aneurysm. Upon heating, the coil collapses to the shape of Fig. 31 to move the mesh 166 to the expanded condition. Heating of the coil may be undertaken in any manner described herein. An advantage of the device 160 is that the device may be heated together with the aneurysm to deploy the device 160 while shrinking the aneurysm. Referring to Fig. 32, another device 160A is shown which is substantially the same as the device 160 except that spring 160A expands in the middle. Fig. 33 shows still another device 160B which has a smaller diameter in the middle to impede fluid flow through the spring 160.

Referring to Fig. 34, another mesh 42A is shown. The mesh 42A may be used with any of the expandable devices described herein and the mechanism for expanding and holding the mesh 42A has been omitted from Fig. 34 for clarity. Any of the actuating and delivery methods and devices described above or any other suitable device may be used with the mesh 42A. The mesh 42A preferably has 10-50 filaments, more preferably 20-50 filaments, extending between first and second ends 150, 152. The filaments 148 are preferably platinum alloy (such as 92% platinum, 8% tungsten). The filaments 148 preferably form a tube in the collapsed position which has a diameter of no more than 0.020 inch but expands to a diameter of at least 0.200 inch at a central portion 154.

The devices described herein are preferably delivered to the aneurysm to occupy the remaining volume of the aneurysm after shrinking the aneurysm. Referring to Figs. 35 and 36, a number of devices 170 may be delivered to the aneurysm with one of the devices 171 being used to heat and shrink the aneurysm. The devices 170 may be

partially or completely insulated in the manner described above to protect the neck while heating and shrinking is accomplished with the device 171. The devices 170 and 171 are shown spaced apart for clarity but, of course, will be closely packed together when filling the aneurysm. The devices 170 and 171 may be any of the expandable devices described
5 herein or any other suitable device without departing from the scope of the invention.

Referring to Fig. 37, another system for reducing the size of an aneurysm is shown. A coil 172 is used to regulate flow of fluid between the aneurysm and the parent vessel. The coil 172 is particularly useful for holding heated fluid in the aneurysm to heat and shrink the aneurysm. The heating device 84 of Figs. 16 and 17, or any other
10 suitable device for heating the aneurysm, is introduced into the aneurysm to heat and shrink the aneurysm. The coil 172 is manipulated by pulling or pushing the coil to retract or deploy the coil 172 from the catheter 8 (see Fig. 1). The pitch of the coil 172 can be varied by pulling or pushing the catheter 8 relative to the coil 172. The windings of the coil 172 may be close together so that the coil 172 substantially impedes flow between
15 the aneurysm and the parent vessel (Fig. 38) or may be spaced-apart to permit slow leakage of fluid into the parent vessel. The coil 172 may be made of any suitable material and is preferably a shape-memory alloy such as nitinol.

Referring to Figs. 39 and 40, another catheter 180 for heating and shrinking an aneurysm is shown. The catheter 180 is preferably less than 5 Fr, more
20 preferably 2-4 Fr, and most preferably about 3 Fr in size so that it is small and flexible enough to shrink select portions of the aneurysm as shown by dotted lines 181 in Fig. 39. The catheter 180 may, of course, be sized larger to shrink larger portions of the aneurysm or other tissue structures. The catheter 180 has a tip 182 which is made of a heat-resistant, non-stick material (such as PTFE) so that the tip can contact the tissue during
25 heating without sticking to the tissue. The catheter 180 may also be a hypotube, guidewire or similar device without departing from the scope of the invention. The tip 182 forms a chamber 183 and has holes 186 formed therein for delivery of a conductive fluid as described below.

The catheter 180 has a lumen 184 which communicates with the chamber
30 183 in the tip 182. The lumen 184 is coupled to the source of fluid 18 (see Fig. 1) which is preferably hypertonic saline. An RF probe 188 passes through the lumen 184 and is coupled to the energy supply 12 (see Fig. 1) which is preferably an RF generator. The RF probe 188 has an electrode 189 positioned in the chamber while a second electrode (not shown) is positioned in contact with the patient's skin in the conventional manner. When

the conductive fluid is delivered through the lumen 184, electrical energy is conducted by the conductive fluid to heat the aneurysm. The holes 183 in the tip 182 may be distributed around the tip 182 (Fig. 39 and 41), positioned at the distal end 185 (Fig. 42) or along the sides 187 (Fig. 43) of the tip 182.

5 After the volume of the aneurysm has been reduced, the aneurysm may be treated in any other manner described herein. Furthermore, the catheter 180 of Figs. 39-43 may be used to heat tissue or fluid in connection with any of the other embodiments described herein and in particular as a substitute for the device 84 of Figs. 16 and 17. Finally, the catheter 180 may be used to heat tissue for any other suitable purpose
10 including those described above. For example, the catheter 180 may be useful in treating venous insufficiency, deep vein reflux or for vein stripping. Furthermore, the catheter 180 may be useful for treating urinary incontinence.

 While the above is a description of the preferred embodiments of the invention, various alternatives, modifications, and equivalents may be used. For example,
15 the expandable device may take any other shape and the sealant may be any other suitable sealant. Furthermore, the dimensions and characteristics of any of the expandable members may be incorporated into any of the other expandable devices described herein without departing from the scope of the invention. Finally, the expandable devices are preferably used when shrinking the aneurysm but the expandable devices may have
20 various features which may be useful when simply filling the aneurysm in the conventional manner.